Deep learning for automatically predicting early haematoma expansion in Chinese patients

Jia-wei Zhong,1 Yu-jia Jin,1 Zai-jun Song,1 Bo Lin,2 Xiao-hui Lu,3 Fang Chen,4 Lu-sha Tong1

ABSTRACT

Background and purpose Early haematoma expansion is deterministic in predicting outcome of intracerebral haemorrhage (ICH) patients. The aims of this study are to develop a novel prediction model for haematoma expansion by applying deep learning model and validate its prediction accuracy.

Methods Data of this study were obtained from a prospectively enrolled cohort of patients with primary supratentorial ICH from our centre. We developed a deep learning model to predict haematoma expansion and compared its performance with conventional non-contrast CT (NCCT) markers. To evaluate the predictability of this model, it was also compared with a logistic regression model based on haematoma volume or the BAT score.

Results A total of 266 patients were finally included for analysis, and 74 (27.8%) of them experienced early haematoma expansion. The deep learning model exhibited highest C statistic as 0.80, compared with 0.64, 0.65, 0.51, 0.58 and 0.55 for hypodensities, black hole sign, blend sign, fluid level and irregular shape, respectively. While the C statistics for swirl sign (0.70; p=0.211) and heterogenous density (0.70; p=0.141) were not significantly higher than that of the deep learning model. Moreover, the predictive value for the deep learning model was significantly superior to that of the logistic model of haematoma volume (0.62; p=0.042) and the BAT score (0.65; p=0.042).

Conclusions Compared with the conventional NCCT markers and BAT predictive model, the deep learning algorithm showed superiority for predicting early haematoma expansion in ICH patients.

INTRODUCTION

Intracerebral haemorrhage (ICH) remains a devastating disease with high mortality and morbidity.1 Early expansion of haematoma is a determinative factor in predicting outcome.2 A wealth of studies has been carried out to seek an advanced way of early identifying patients with haematoma expansion. Spot sign was a well-established imaging marker associated with haematoma expansion, based on CT angiography (CTA).3–5 However, in large-scaled clinical trials, the majority of ICH patients did not undergo CTA when admitted.6 Imaging signs more feasible based on non-contrast CT (NCCT) included black hole sign, swirl sign, island sign, blend sign and so on.7–10 However, these signs usually bared a poor sensitivity since their probability of occurrence is relatively low.11 12 Recently, multi-itemed scores for predicting haematoma expansion expansion have been proposed in order to increase prediction efficacy, such as the BRAIN (B for baseline ICH volume, R for recurrent ICH, A for anticoagulation with warfarin, I for intraventricular haemorrhage and N for numbers of hours from onset to CT), HEAVN (H for heterogenity, E for peripheral edema, A for anticoagulation use, V for volume>30ml on initial CT, and N for Niveau formation), BAT (B for blend sign, A for hypodensity presence, and T for time from onset to NCCT). Yet none of these scores exhibits a C statistic >0.8, which means unsatisfactory prediction value.12

Nowadays, deep learning is recognised as the most effective machine learning algorithm and is cutting a striking figure in processing multi-categorical data. Some predicting models based on deep learning have been successfully used to predict clinical outcome. Convolutional neural networks (CNN) is a deep learning statistical method commonly used in image recognition.13 U-net is a network and training strategy which relies on strong usage of data augmentation, and thereby requires fewer data and shorter time to produce an ideal method.14 We hypothesised that CNN-derived U-net-supported modelling based on topological and morphological imaging features on NCCT might provide an advanced predicting model which retains both better prediction efficacy and convenient clinical application. For this purpose, a novel prediction model for ICH patients with early haematoma expansion is developed and tested compared with NCCT signs, as well as haematoma volume and BAT score.
METHODS

The data that support the findings of the study are available from the corresponding author on reasonable request. Retrospective analysis of a prospectively and consecutively collected cohort of spontaneous ICH patients in The Second Affiliated Hospital of Zhejiang University between February 2012 to October 2019. Patients were enrolled if they: (1) were over 18 years old, (2) were obtained baseline CT imaging within 8 hours from onset and (3) obtained follow-up CT scan after 20–24 hours after baseline. We excluded patients with infratentorial haematoma, ventricular haemorrhage only, critical deterioration or surgical operation before the follow-up CT imaging or poor image quality. From the prospectively longitudinal cohort, patients between February 2012 and August 2018 were selected for training dataset and those between September 2018 and October 2019 were selected as testing dataset. Early haematoma expansion was defined as an increase of >6 mL absolute volume or 33% relative volume of haematoma in the follow-up CT compared with initial CT.

Labelling and calculating the volume of haematoma

The baseline CT images for this study were obtained with four different CT scanners. The acquisition parameters were described in online supplemental table 1. Manual segmentations for haematoma were performed on the CT scans by a single radiologist with more than 10 years of experience, and 20 randomly selected cases were re-evaluated after a minimal interval of 7 days by another skilled radiologist to assess inter-rater reliability. The inter-rater agreement for the segmentation of haematoma was 0.978 for semi-automated segmentation method. Based on the binary label map, the haematoma volume was then calculated.

Assessment of the NCCT markers and the BAT score

The NCCT signs were evaluated by two authors, each with >10 years of experience. The inter-rater reliability was assessed using the whole dataset with a dichotomy (κ=0.886, 0.906, 0.848, 0.951, 0.892, 0.859, 0.932 for hypodensities, black hole sign, swirl sign, blend sign, fluid level, irregular shape, heterogeneous density, respectively). In addition, disagreements were settled by consensus between the two authors. The BAT score was based on the assessment of NCCT markers. The process of assessing the NCCT markers and the BAT score was shown in online supplementa tables 2 and 3.

Data preprocessing and augmentation

The baseline CT images were skull stripped and then normalised for signal intensity. The images were all resampled to a uniform field of view of 112×112×160 mm and matrix size of 256×256×32. Considering the limited data size, data augmentation was performed via three-dimensional rotation, translation and scaling. Thereby the size of original dataset was augmented 10-fold (see online supplemental file.

Training of the deep learning model

A two-output deep learning model was designed to segment the haematoma to acquire high-level imaging features and predict early haematoma expansion.

Figure 1 The concept of the model in this study: (1) the model had a single input (CT imaging data) and two outputs for segmentation and prediction; (2) based on the U architecture, the high-level image information derived from the bridge layer of U were treated as biomarkers for haematoma expansion prediction.
U-net provides technical support for basic architecture design for segmentation. The most aggregated contextual information was deposited in the middle layer of the model (the deepest convolutional layer of the U) and extracted as the high-level imaging feature used for a binary classification for haematoma expansion (figure 1). Detail of the model architecture is shown in online supplemental figure 1. For training, fivefold cross-validation was used for adjusting hyperparameters. These processes only involved CT data. No clinical information was applied as input. See online supplemental file.

Logistic regression models based on the haematoma volume and the BAT score

To compare the performance of the deep learning model, univariate logistic regression models were respectively developed based on the haematoma volume and the BAT score from the training dataset.

Evaluation of the models

Each model was applied in the testing dataset. The sensitivity, specificity, likelihood ratio and receiver operator characteristic (ROC) area under the curve (AUC) were calculated for each model and NCCT markers. Dice coefficient was calculated to evaluate the performance of segmentation.

Statistical analysis

Continuous variables are expressed as the mean with the CI of the mean or SD, or as the median with IQR. Continuous variables were compared using Mann-Whitney U test and Student’s t-test as appropriate, and categorical variables were compared using Pearson’s χ² test. AUC of deep learning model was compared with that of the other models and NCCT signs using Delong test. The statistical analysis was performed with R statistical software (V.4.0.1).

RESULTS

A total of 317 patients fulfilled our inclusion criteria. Fifty-one patients were excluded due to the following reasons, infratentorial haematoma (n=29), only ventricular haemorrhage (n=3), died or had surgical operation before follow-up CT (n=11), or with poor image quality (n=8). A total of 266 patients were included for analysis, and divided into training dataset (n=189) and testing dataset (n=77) according to the admission date (figure 2). Baseline patient characteristics were compared between the training and testing dataset in table 1.

![Figure 2](http://svn.bmj.com/) Flow chart illustrating patient selection for training dataset and testing dataset.
The Dice coefficient of the CNN model was 0.96±0.01 with the training dataset and 0.87±0.15 with the testing dataset. Representative images are shown in figure 3.

Of the 266 patients, 74 (27.8%) patients had haematoma expansion. Patients of training dataset and testing dataset were not different in the haematoma volume (p=0.850) and the BAT score (p=0.065). The sensitivity, specificity, likelihood ratio and AUCs of the NCCT markers and the three models were shown in table 2, and the ROC curves were shown in online supplemental figure 2.

For the NCCT markers, the CNN model exhibited highest AUC: 0.80 (95% CI 0.70 to 0.90) compared with 0.64 (95% CI 0.55 to 0.75), 0.65 (95% CI 0.54 to 0.75), 0.51 (95% CI 0.41 to 0.61), 0.58 (95% CI 0.48 to 0.67) and 0.55 (95% CI 0.44 to 0.67) for hypodensities, black hole sign, blend sign, fluid level and irregular shape, while the AUCs of swirl sign (0.70 (95% CI 0.61 to 0.80); p=0.211) and heterogeneous density (0.70 (95% CI 0.59 to 0.81); p=0.141) were not significantly higher than that of the deep learning model. For the three models, the CNN model showed superior predictive accuracy than the haematoma volume (AUC 0.62 (95% CI 0.46 to 0.78); p=0.042) and the BAT score (0.65 (95% CI 0.53 to 0.78); p=0.042) according to logistic regression models. In addition, the CNN model represented the lowest negative likelihood ratio (0.06 (95% CI 0.02 to 0.24)).

**DISCUSSION**

In this study, we developed a CNN-derived predictive model based on topological and morphological imaging features on NCCT to predict early haematoma expansion in ICH patients. According to the sensitivity, specificity, positive likelihood ratio, negative likelihood ratio and C statistics, comparing with other existing prediction models or NCCT markers, CNN model exhibited superior prediction efficacy.

Most recently, several NCCT markers were proposed for predicting early haematoma expansion in ICH patients, including blend sign, swirl sign and black hole sign. 7 8 10

**Table 2** Scores for models and NCCT markers of testing dataset

<table>
<thead>
<tr>
<th></th>
<th>Sensitivity</th>
<th>Specificity</th>
<th>Positive likelihood ratio*</th>
<th>Negative likelihood ratio*</th>
<th>AUC</th>
<th>P value†</th>
</tr>
</thead>
<tbody>
<tr>
<td>Hypodensities</td>
<td>0.77 (0.54 to 0.91)</td>
<td>0.51 (0.37 to 0.64)</td>
<td>0.63 (0.40 to 0.98)</td>
<td>0.18 (0.08 to 0.40)</td>
<td>0.64 (0.53 to 0.75)</td>
<td>0.026</td>
</tr>
<tr>
<td>Black hole sign</td>
<td>0.36 (0.18 to 0.59)</td>
<td>0.93 (0.82 to 0.98)</td>
<td>2.00 (0.82 to 4.89)</td>
<td>0.27 (0.17 to 0.44)</td>
<td>0.65 (0.54 to 0.75)</td>
<td>0.006</td>
</tr>
<tr>
<td>Swirl sign</td>
<td>0.86 (0.64 to 0.96)</td>
<td>0.54 (0.41 to 0.68)</td>
<td>0.76 (0.50 to 1.16)</td>
<td>0.1 (0.03 to 0.30)</td>
<td>0.70 (0.61 to 0.80)</td>
<td>0.211</td>
</tr>
<tr>
<td>Blend sign</td>
<td>0.18 (0.06 to 0.41)</td>
<td>0.84 (0.71 to 0.92)</td>
<td>0.44 (0.18 to 1.08)</td>
<td>0.39 (0.26 to 0.59)</td>
<td>0.51 (0.41 to 0.61)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Fluid level</td>
<td>0.23 (0.09 to 0.46)</td>
<td>0.93 (0.82 to 0.98)</td>
<td>1.25 (0.49 to 3.19)</td>
<td>0.33 (0.22 to 0.51)</td>
<td>0.58 (0.48 to 0.67)</td>
<td>0.002</td>
</tr>
<tr>
<td>Irregular shape</td>
<td>0.73 (0.50 to 0.88)</td>
<td>0.38 (0.261 to 0.52)</td>
<td>0.47 (0.30 to 0.74)</td>
<td>0.29 (0.14 to 0.59)</td>
<td>0.55 (0.44 to 0.67)</td>
<td>0.002</td>
</tr>
<tr>
<td>Heterogeneous density</td>
<td>0.73 (0.50 to 0.88)</td>
<td>0.67 (0.53 to 0.79)</td>
<td>0.89 (0.55 to 1.43)</td>
<td>0.16 (0.08 to 0.34)</td>
<td>0.70 (0.59 to 0.81)</td>
<td>0.141</td>
</tr>
<tr>
<td>Haematoma Volume</td>
<td>0.50 (0.29 to 0.71)</td>
<td>0.84 (0.71 to 0.92)</td>
<td>1.22 (0.65 to 2.29)</td>
<td>0.24 (0.14 to 0.41)</td>
<td>0.62 (0.46 to 0.78)</td>
<td>0.042</td>
</tr>
<tr>
<td>BAT score</td>
<td>0.36 (0.18 to 0.59)</td>
<td>0.76 (0.62 to 0.86)</td>
<td>0.61 (0.32 to 1.17)</td>
<td>0.33 (0.21 to 0.53)</td>
<td>0.65 (0.53 to 0.78)</td>
<td>0.042</td>
</tr>
<tr>
<td>CNN</td>
<td>0.91 (0.69 to 0.98)</td>
<td>0.58 (0.44 to 0.71)</td>
<td>0.87 (0.57 to 1.33)</td>
<td>0.06 (0.02 to 0.24)</td>
<td>0.80 (0.70 to 0.90)</td>
<td>N/A</td>
</tr>
</tbody>
</table>

*Positive likelihood ratio and negative likelihood ratio were weighted by prevalence.
†AUC of CNN model was compared with AUC of the other models and NCCT signs using Delong test.
AUC, receiver operator characteristic area under the curve; CNN, convolutional neural network; N/A, not applicable; NCCT, non-contrast CT.
However, most of the NCCT markers were with relatively low sensitivity and low incidence. To improve the performance of NCCT markers, Morotti et al reported the BAT score based on the NCCT signs, and shown that their BAT score had a C-statistic of 0.65–0.70 for validation cohorts, which was in accordance with results of this study. Size of their dataset was sufficiently large, whereas, the comparison between the BAT score and the conventional NCCT markers was not performed. In addition, correlations between the initial haematoma volume and early haematoma expansion have been reported. Therefore, in the present study, the logistic model only after a bundle of clinical information was required as the input for haematoma growth with an external validation AUC of 0.85. Support vector machine (SVM) to predict early haematoma expansion in intracerebral hemorrhage: definition, prevalence, reliability and prognostic value. Neurology 2011;76:1238–44.

The study was approved by the Institutional Review Board of The Second Affiliated Hospital of Zhejiang University. Ethics approval Not commissioned; externally peer reviewed.

Data availability statement The data that support the findings of the study are available from the corresponding author upon reasonable request.

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REFERENCES

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Patient consent for publication Not required.

Ethics approval This study was approved by the Institutional Review Board of The Second Affiliated Hospital of Zhejiang University.

Provenance and peer review Not commissioned; externally peer reviewed.

Data availability statement The data that support the findings of the study are available from the corresponding author upon reasonable request.

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REFERENCES
SUPPLEMENTAL MATERIAL

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Image acquisition

The baseline CT images from our study were obtained with four CT scanners: GE Optima CT540, SIEMENS SOMATOM Definition Flash, SIEMENS SOMATOM Force, SIEMENS SOMATOM Perspective. The acquisition parameters were as follows: slice thickness, 5.0mm; axial slice number, 27-34; voxel size, 0.3906-0.5566×0.3906-0.5566×5.0mm; matrix size, 512×512; field of view, 200-285×200-285mm; window width, 90HU; window level, 35HU (Supplemental Table1).

Labeling and calculation of the hematoma volume

Manual segmentations for hematoma were performed on the CT scans by a single author with more than 10 years of experience. To assess interrater reliability, repeat manual segmentations in 20 randomly selected cases were performed after a minimal interval of 7 days. Labels were manually painted on each 2-dimensional slice of each CT image applying the open-source software ITK-SNAP[1] (http://www.itksnap.org/). Comparing to the contralateral hemisphere, intracerebral hemorrhage was differentiated from intraventricular hemorrhage or subarachnoid hemorrhage. Based on the binary label map, the hematoma volume was then calculated.

Data preprocessing

The CT images of our study were collected as a Digital Imaging and Communication in Medicine (DICOM) image series, and then were transformed to Neuroimaging Informatics Technology Initiative format. Each CT image was skull skipped by using Otsu’s method.[2] The CT images were resampling to a field of view of 112 × 112 × 160 mm and matrix size of 256 × 256 × 32 by applying a bicubic interpolation algorithm, and then the images were windowed with a threshold of 0 to 100 HU. After this, normalization was performed by subtracting the mean value within the skull-stripped brain region and dividing by the standard deviation of the signal intensity of the region, and negative values were set to zero.
Data augmentation

Data augmentation were performed by applying 3-dimensional image transformation with scaling, translation, and rotation. For the training dataset, each CT image was randomly transformed by applying these three transformations using a linear interpolation algorithm. The scaling and translation were performed between –10% and 10% of the image size and the rotation between –5 and 5 degrees. The size of the training dataset was increased 10 times with these techniques.

Model architecture

In this study, we build a two-task model based on a deep convolution neural network. The semantic segmentation of hematoma and the prediction of hematoma expansion were simultaneously working. Hematoma expansion outcome was binarized according to the volume of 24h follow-up CT image compared to the baseline CT image(≥6 mL or ≥33%). Detail of the model architecture is shown in Supplemental Figure 1.

Segmentation network

The segmentation network was based on U-Net[3], an encoder-decoder network for 3-dimensional image segmentation. Our network for segmentation had 4-level architecture with 2 down-sampling, 2 up-sampling and 1 convolution operation for bridging layer(Supplemental Figure 2): 32 × 256 × 256 (16 channels) → 16 × 128 × 128 (32 channels) → 8 × 64 × 64 (64 channels) → 8 × 64 × 64 (128 channels) → 16 × 128 × 128 (64 channels) → 32 × 256 × 256 (32 channels). The down-sampling of encoding path was performed by a 3 × 3 × 3 three-dimensional convolution layer with 2 × 2 × 2 strides, and the up-sampling of decoding path was performed with a size of 2 × 2 × 2. Padding was applied in steps above. The final output of segmentation was performed by applying 1 × 1 × 1 convolution with sigmoid function, reducing the channel number to one.

Classification network

The classification network was added to the bridging layer of the segmentation network (Supplemental Figure 1). Two 3 × 3 × 3(with 128 filters) three-dimensional convolution operations with padding were performed and then feature channels(size 128 × 8 × 64 × 64) were processed with three-dimensional global average pooling to be 128 units. The flattened features were connected to a unit of output applying the Sigmoid activation function for the binary classification work.
Training process

The deep neural network model had 3,802,578 parameters. The Adam optimizer was applied with back propagation. The loss function for segmentation was Dice loss (1 – Dice coefficient), and the loss function for classification was binary cross-entropy. The segmentation and classification were simultaneously trained with the cost function in the ratio 9:1 (segmentation: classification). The network was trained for 40 epochs totally with a batch size of 1. A multi-step learning rate schedule was performed with an initial learning rate of $1 \times 10^{-4}$, reduced by a factor of 10 at 20th and 30th epoch.

The training process was performed with an 11-GB graphics processing unit (NVIDIA GeForce RTX 2080Ti). Training process took about 14 hours. The code of convolution neural network was written in Python 3.7 (https://www.python.org/) and implemented in open-source deep learning framework Pytorch 1.4.0 (https://pytorch.org/).

Model evaluation

For the segmentation task, the Dice coefficient was calculated to evaluate the segmentation results.

For the classification task, the sensitivity, specificity, likelihood ratio weighted by prevalence, and area under the curve (AUC) were calculated based on receiver operating characteristic (ROC) curves (Supplemental Figure 2).

Figures and Tables

Supplemental Table 1 Acquisition parameters for CT scanners

<table>
<thead>
<tr>
<th>Scanner</th>
<th>GE Optima CT540</th>
<th>SIEMENS SOMATOM Definition Flash</th>
<th>SIEMENS SOMATOM Force</th>
<th>SIEMENS SOMATOM Perspective</th>
</tr>
</thead>
<tbody>
<tr>
<td>Slice thickness, mm</td>
<td>5.0</td>
<td>5.0</td>
<td>5.0</td>
<td>5.0</td>
</tr>
<tr>
<td>Axial slice number</td>
<td>28~34</td>
<td>26~28</td>
<td>27</td>
<td>27</td>
</tr>
<tr>
<td>Voxel size, mm</td>
<td>0.4883×5.0</td>
<td>0.3906-0.5566×5.0</td>
<td>0.3906-0.4453×5.0</td>
<td>0.4492×0.4492×5.0</td>
</tr>
<tr>
<td>Matrix size</td>
<td>512×512</td>
<td>512×512</td>
<td>512×512</td>
<td>512×512</td>
</tr>
<tr>
<td>Field of view, mm</td>
<td>250×250</td>
<td>200-285×200-285</td>
<td>200-228×200-228</td>
<td>230×230</td>
</tr>
<tr>
<td>Window width</td>
<td>90</td>
<td>90</td>
<td>90</td>
<td>90</td>
</tr>
<tr>
<td>Window level</td>
<td>35</td>
<td>35</td>
<td>35</td>
<td>35</td>
</tr>
</tbody>
</table>
CT indicates computed tomography.

**Supplemental Table 2 Diagnostic criteria for NCCT markers**[4]

<table>
<thead>
<tr>
<th>Marker</th>
<th>Criteria</th>
</tr>
</thead>
<tbody>
<tr>
<td>Hypodensity</td>
<td>Any hypodense region strictly encapsulated within the hemorrhage with any shape, size, and density.</td>
</tr>
<tr>
<td>Black hole sign</td>
<td>Hypoattenuating area with a density difference &gt;28HU compared with the surrounding hematoma. No connection with surface outside the hematoma.</td>
</tr>
<tr>
<td>Swirl sign</td>
<td>Rounded, streak-like, or irregular region of hypo- or isoattenuation compared with the brain parenchyma. Does not have to be encapsulated in the ICH.</td>
</tr>
<tr>
<td>Blend sign</td>
<td>Relatively hypoattenuating area next to a hyperattenuating area of the hematoma, with a well-defined margin and a density difference &gt;18HU between the two areas.</td>
</tr>
<tr>
<td>Fluid level</td>
<td>Presence of an area hypodense to the brain above and one hyperattenuating area below a discrete straight line of separation, irrespective of its density appearance.</td>
</tr>
<tr>
<td>Irregular shape</td>
<td>Two or more focal hematoma margin irregularities, joined or separate from the hematoma edge on the axial NCCT slice with largest hematoma area.</td>
</tr>
</tbody>
</table>

NCCT indicates non-contrast computed tomography.

**Supplemental Table 3 Criteria for the BAT score**[5]

<table>
<thead>
<tr>
<th>Points</th>
<th>Blend sign</th>
<th>Any hypodensity</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Present</td>
<td>Present</td>
</tr>
<tr>
<td>1</td>
<td>Absent</td>
<td>Absent</td>
</tr>
<tr>
<td>0</td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

NCCT indicates non-contrast computed tomography.

**Supplemental Figure 1 The architecture of the model**
Supplemental Figure 2 ROC curves of testing

The receiver operating characteristic curves of the CNN model, the hematoma volume model and the BAT score model were displayed.

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In this study, we build a two-task model based on a deep convolution neural network. The semantic segmentation of hematoma and the prediction of hematoma expansion were simultaneously working. Hematoma expansion outcome was binarized according to the volume of 24h follow-up CT image compared to the baseline CT image(≥6 mL or ≥33%). Detail of the model architecture is shown in Supplemental Figure 1.

Segmentation network

The segmentation network was based on U-Net[3], an encoder-decoder network for 3-dimensional image segmentation. Our network for segmentation had 4-level architecture with 2 down-sampling, 2 up-sampling and 1 convolution operation for bridging layer(Supplemental Figure 2): 32 × 256 × 256 (16 channels) → 16 × 128 × 128 (32 channels) → 8 × 64 × 64 (64 channels) → 8 × 64 × 64 (128 channels) → 16 × 128 × 128 (64 channels) → 32 × 256 × 256 (32 channels). The down-sampling of encoding path was performed by a 3 × 3 × 3 three-dimensional convolution layer with 2 × 2 × 2 strides, and the up-sampling of decoding path was performed with a size of 2 × 2 × 2. Padding was applied in steps above. The final output of segmentation was performed by applying 1 × 1 × 1 convolution with sigmoid function, reducing the channel number to one.

Classification network

The classification network was added to the bridging layer of the segmentation network (Supplemental Figure 1). Two 3 × 3 × 3(with 128 filters) three-dimensional convolution operations with padding were performed and then feature channels(size 128 × 8 × 64 × 64) were processed with three-dimensional global average pooling to be 128 units. The flattened features were connected to a unit of output applying the Sigmoid activation function for the binary classification work.
Training process

The deep neural network model had 3,802,578 parameters. The Adam optimizer was applied with back propagation. The loss function for segmentation was Dice loss (1 – Dice coefficient), and the loss function for classification was binary cross-entropy. The segmentation and classification were simultaneously trained with the cost function in the ratio 9:1 (segmentation: classification). The network was trained for 40 epochs totally with a batch size of 1. A multi-step learning rate schedule was performed with an initial learning rate of $1 \times 10^{-4}$, reduced by a factor of 10 at 20th and 30th epoch.

The training process was performed with an 11-GB graphics processing unit (NVIDIA GeForce RTX 2080Ti). Training process took about 14 hours. The code of convolution neural network was written in Python 3.7(https://www.python.org/) and implemented in open-source deep learning framework Pytorch 1.4.0(https://pytorch.org/).

Model evaluation

For the segmentation task, the Dice coefficient was calculated to evaluate the segmentation results.

For the classification task, the sensitivity, specificity, likelihood ratio weighted by prevalence, and area under the curve (AUC) were calculated based on receiver operating characteristic (ROC) curves (Supplemental Figure 2).

Figures and Tables

Supplemental Table 1 Acquisition parameters for CT scanners

<table>
<thead>
<tr>
<th>Scanner</th>
<th>GE Optima CT540</th>
<th>SIEMENS SOMATOM Definition Flash</th>
<th>SIEMENS SOMATOM Force</th>
<th>SIEMENS SOMATOM Perspective</th>
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</thead>
<tbody>
<tr>
<td>Slice thickness, mm</td>
<td>5.0</td>
<td>5.0</td>
<td>5.0</td>
<td>5.0</td>
</tr>
<tr>
<td>Axial slice number</td>
<td>28~34</td>
<td>26~28</td>
<td>27</td>
<td>27</td>
</tr>
<tr>
<td>Voxel size, mm</td>
<td>0.4883×0.4883×5.0</td>
<td>0.3906–0.5566×0.3906–0.5566×5.0</td>
<td>0.3906–0.4453×0.3906–0.4453×5.0</td>
<td>0.4492×0.4492×5.0</td>
</tr>
<tr>
<td>Matrix size</td>
<td>512×512</td>
<td>512×512</td>
<td>512×512</td>
<td>512×512</td>
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<tr>
<td>Window width</td>
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<td>90</td>
<td>90</td>
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</tr>
<tr>
<td>Window level</td>
<td>35</td>
<td>35</td>
<td>35</td>
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</tr>
</tbody>
</table>
CT indicates computed tomography.

**Supplemental Table 2 Diagnostic criteria for NCCT markers [4]**

<table>
<thead>
<tr>
<th>Marker</th>
<th>Criteria</th>
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</thead>
<tbody>
<tr>
<td>Hypodensity</td>
<td>Any hypodense region strictly encapsulated within the hemorrhage with any shape, size, and density.</td>
</tr>
<tr>
<td>Black hole sign</td>
<td>Hypoattenuating area with a density difference &gt;28HU compared with the surrounding hematoma. No connection with surface outside the hematoma.</td>
</tr>
<tr>
<td>Swirl sign</td>
<td>Rounded, streak-like, or irregular region of hypo- or isoattenuation compared with the brain parenchyma. Does not have to be encapsulated in the ICH.</td>
</tr>
<tr>
<td>Blend sign</td>
<td>Relatively hypoattenuating area next to a hyperattenuating area of the hematoma, with a well-defined margin and a density difference &gt;18HU between the two areas.</td>
</tr>
<tr>
<td>Fluid level</td>
<td>Presence of an area hypodense to the brain above and one hyperattenuating area below a discrete straight line of separation, irrespective of its density appearance.</td>
</tr>
<tr>
<td>Irregular shape</td>
<td>Two or more focal hematoma margin irregularities, joined or separate from the hematoma edge on the axial NCCT slice with largest hematoma area.</td>
</tr>
</tbody>
</table>

NCCT indicates non-contrast computed tomography.

**Supplemental Table 3 Criteria for the BAT score [5]**

<table>
<thead>
<tr>
<th>Points</th>
<th></th>
<th></th>
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</thead>
<tbody>
<tr>
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<td></td>
<td></td>
</tr>
<tr>
<td>Present</td>
<td>1</td>
<td></td>
</tr>
<tr>
<td>Absent</td>
<td>0</td>
<td></td>
</tr>
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</table>

Any hypodensity

<table>
<thead>
<tr>
<th>Points</th>
<th></th>
</tr>
</thead>
<tbody>
<tr>
<td>Present</td>
<td>2</td>
</tr>
<tr>
<td>Absent</td>
<td>0</td>
</tr>
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</table>

Time from onset to NCCT

<table>
<thead>
<tr>
<th>Points</th>
<th></th>
</tr>
</thead>
<tbody>
<tr>
<td>&lt;2.5h</td>
<td>2</td>
</tr>
<tr>
<td>≥2.5h</td>
<td>0</td>
</tr>
</tbody>
</table>

NCCT indicates non-contrast computed tomography.

**Supplemental Figure 1 The architecture of the model**
Supplemental Figure 2 ROC curves of testing

The receiver operating characteristic curves of the CNN model, the hematoma volume model and the BAT score model were displayed.

References